EEG-Based Prediction of Driver Takeover Performance

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ABSTRACT

In the context of conditional autonomous driving, ensuring a safe takeover is of paramount importance. While previous studies have delved into factors influencing drivers' takeover performance, there remains a gap in research concerning the development of performance models capable of predicting takeover quality. To address this challenge, this study focuses on predicting driver takeover performance before the issuance of a takeover request based on Electroencephalogram (EEG) features. For this purpose, 72 subjects were recruited to participate in a driving simulation experiment, responding to a total of eight takeover events. Both their EEG signals and driving performance data were recorded. The takeover performance was subsequently categorized as high, medium, or low quality through a subjective review of the takeover process videos. A total of 480 EEG features, such as the power of α band, were extracted. Five machine learning models: Decision Trees (DT), Support Vector Machine (SVM), Random Forest (RF), Light Gradient Boosting Machine (LightGBM), and Multi-layer Perceptron (MLP), were utilized to develop the takeover performance prediction models. The results showed that the LightGBM model outperformed others, achieving an accuracy of 84.2% and an F1 score of 83.0%. In contrast, the DT model demonstrated the lowest performance, with an accuracy of 59.4% and an F1 score of 57.8%. This study underscores the potential of machine learning models in predicting driver takeover performance, thereby contributing to the advancement of machine learning applications in the field of autonomous driving.

Keywords: Autonomous driving, Takeover performance, EEG, Machine learning, Predictive modeling

INTRODUCTION

With the rapid development of autonomous driving technology, this field holds immense potential in improving road safety, reducing traffic accidents, alleviating traffic congestion, and enhancing environmental benefits. However, it also faces new challenges. One such challenge is the takeover transition in conditional autonomous driving (Zhou, Yang and Zhang, 2019). The Society of Automotive Engineers (SAE) in the United States has defined autonomous driving cars into six levels (SAE, 2018). According to this definition, drivers of Level 3 autonomous driving do not need to continuously monitor the driving environment and system performance (Naujoks, Purucker and Neukum, 2016). The driver is only required to take over control of the vehicle when the vehicle encounters situations that the system cannot handle or when the automatic system fails. This is done by issuing auditory, visual, or tactile Takeover Request (TOR) to remind the driver to promptly resume manual driving (Wan and Wu, 2018).

The transition from autonomous driving to manual driving has received widespread attention. To facilitate takeover transitions, researchers have delved deeply into various factors affecting driver takeover performance, including the cognitive and emotional states of drivers when performing Non-Driving Related Tasks (NDRTs) (Du et al., 2020a), and their performance under different driving environments (Li et al., 2018). Drivers being in complex traffic environments and participating in NDRTs may lead to a decline in their attention, reducing the ability to correctly control automated systems, thereby posing a hidden danger to driving safety. In this sense, the prediction of takeover quality in L3 autonomous driving is necessary for safe takeover.

Research on predicting driver takeover performance using Machine Learning and Deep Learning algorithms is increasingly gaining attention. For instance, Braunagel, Rosenstiel, and Kasneci (2017) developed an automated system that classifies the driver's takeover readiness into low and high, with the best result based on the SVM classifier achieving an accuracy of 79%. Deo and Trivedi (2020) proposed a Long Short-Term Memory (LSTM) model for continuously estimating the driver's takeover readiness index, with their best result achieving a Mean Absolute Error (MAE) of 0.449 in a 5-point takeover readiness index. Du et al. (2020b) used the driver's takeover performance into good and bad using the RF model, with the best accuracy reaching 84.3%.

In summary, many studies have conducted case analyses around the relationship between takeover time and quality. However, fewer studies have focused on takeover performance modeling and prediction, and there are still some research gaps to be addressed. Firstly, although existing research has explored the relationship between ECG and EDA physiological signals and eye movement behavior with takeover performance, it is still unclear whether EEG signals can be used to predict driver performance during interactions with Autonomous Vehicles. Secondly, the exploration of machine learning methods in this field is limited. It is currently unclear whether better evaluation models can be developed by exploring various machine learning algorithms. This study aims to collect EEG signals and compare the results of various machine learning takeover performance evaluation models to address the aforementioned research gaps, which will help to better understand the relationship between physiological signals and driving takeover, and better develop potential applications of driving assistance systems.

EXPERIMENT DESIGN

Experiment Subject

For the driving experiment, we recruited a diverse group of 72 participants, evenly split with 36 males and 36 females. The participants were young adults, with an average age of 22.6 years (standard deviation = 1.6), and ages ranging from 18 to 28 years. Each participant was a licensed driver with

either normal or corrected-to-normal vision. To ensure their optimal health status for the experiment, they were instructed to abstain from any drugs or alcohol for at least 24 hours prior to the experiment.

Experiment Equipment

Figure 1 provides an overview of the driving simulator, a Huawei MatePad Pro tablet, and the EEG recording device used in this experiment. The driving simulator includes three 27-inch LED monitors, a high-performance computer, a Logitech steering wheel, brake and accelerator pedals, and a driver's seat. The simulator is equipped with UC-Win/Road software, which offers various driving scenarios and records driving data at a frequency of 60Hz. The simulator can operate in manual or automatic mode, and a start/stop button for the autonomous driving function is installed on the steering wheel. The Huawei MatePad Pro tablet, with a screen size of 10.8 inches, is placed on the right side of the steering wheel, simulating the position of the central control panel in actual vehicles.

The EEG signals of the experiment participants were collected through ANT Neuro. It has 32 EEG channels and records EEG signals at a frequency of 500Hz. The placement of the electrodes follows the international 10–20 system. To ensure the best signal quality, the contact impedance between the electrodes and the participant's skin is kept below 20 k Ω .



Figure 1: EEG and other equipment used in the experiment.

Experiment Design

The experiment adopted a mixed design of gender (male vs. female, betweensubject variable) \times eight TOR scenarios (4 types of hazards \times 2 levels of road curvature, within-subject variable). A two-way 95-kilometer-long road was created for the experiment, with three lanes in each direction, to simulate urban driving scenarios. Participants were instructed to maintain their position in the middle lane. TOR would be triggered when the autonomous driving system could not handle an upcoming hazard, necessitating the transfer of vehicle control to the driver. The experiment developed eight TOR scenarios, with four types of hazards being a broken-down vehicle, road construction, pedestrian crossing, and landslide, and two types of road curvature being a straight road and a sharp turn with a radius of 200 meters. As shown in Figure 2, participants initially drove in autonomous mode, with the system maintaining a constant speed of 100 kilometers per hour. Participants were free to perform NDRT of their choice, with the NDRT in this experiment being a typing task, primarily serving as a visual manual interference, where participants needed to accurately input the displayed Chinese characters on a tablet computer. In most cases, the TOR was presented in a standardized format, triggered when the participant's vehicle was approximately 10 seconds away from an obstacle. The TOR included a 75-decibel sine sound (2010 Hz, duration 0.47 seconds) and a red text prompt displayed in the lower area of the windshield. At the start of the TOR, participants needed to press the X button on the steering wheel, switch to manual driving, and handle the imminent obstacle.



Figure 2: Diagram of experimental design.

Experimental Procedure

Upon arrival at the experimental site, the participants completed a demographic questionnaire and were briefly introduced to the purpose and procedure of the experiment. Subsequently, they read and signed an informed consent form. Next, they underwent a 10–15 minutes driving practice session, which primarily included: manually driving the vehicle and accelerating to 120 km/s, quick lane changes, emergency braking, turning corners, switching to autonomous driving mode, taking over the vehicle and avoiding hazards, etc. In addition, the participants familiarized themselves with the secondary task of typing on a tablet and completed a combination of the tablet typing task and vehicle takeover. Afterwards, the participants put on an EEG cap and began the official driving phase. Throughout the entire experiment, they were required to comply with road traffic regulations and TOR. The entire experiment lasted approximately 60 minutes.

MODELING OF TAKEOVER PERFORMANCE

EEG data were collected for this study. However, due to technical issues with the driving simulator and physiological sensors, the data from 3

participants had to be excluded. Consequently, we were left with usable data from 69 participants for further analysis. The raw data underwent preprocessing, followed by feature extraction and selection, as well as the establishment of ground truth. Following this, a five-fold cross-validation method was employed to adjust the hyperparameters, train the model, and make predictions. The predicted results were then compared with the actual results.

Data Pre-Processing

For the EEG data, this study first applied a zero-phase Finite Impulse Response (FIR) band-pass filter, selecting a frequency range of 0.5Hz-30Hz, to eliminate noise and unwanted frequency components. Following this, the Krutosis function was used to automatically check for bad leads, and the Spherical function was used to interpolate these bad leads. Subsequently, Independent Component Analysis (ICA) was employed to decompose the EEG signals, identify artifacts and noise such as electrooculography and electromyography, and manually remove them. After completing these steps, the EEG signals were re-referenced and downsampled, reducing the sampling rate to 100Hz. These processing steps were carried out to ensure the quality and accuracy of the signals.

Feature Generation

By comparing the modeling results of different time periods, data from X seconds before the TOR was issued to the time the TOR was issued was selected for feature extraction. The values of X were 5, 7, 10, 15, 20, 30, 40, 50, and 60. Using one-way ANOVA, it was found that the modeling accuracy was best with a 20-second time window (F (8,1926) = 298.7, p <0.001). Referring to the research of Du et al. (2020b) and Alambeigi et al. (2023), this study chose a sliding time window size of 3s with an overlap rate of 67% (i.e., a step size of 1s) to slice the data for each scenario time period.

Scholars in the field of data science seem to believe that data clustering can improve the quality of classification (Khan, 2017). Some research suggests using the original features in combination with the features generated by clustering (Piernik and Morzy, 2021), as this can simplify the model by combining the features after clustering, reduce the risk of overfitting, improve robustness against outliers, and retain all the information of the original features. This study found that using the original features in combination with the clustering features can improve model performance.

This study used EEG data and calculated frequency domain features, including the amplitude (AMP) and power spectral density (PSD) of δ waves (1–4Hz), θ waves (4–8Hz), α waves (8–13Hz), and β waves (13–30Hz). Therefore, a total of 8 frequency domain features were obtained (4 frequency bands × 2 features). Since there are 32 channels in the whole brain, excluding the M1 and M2 reference electrodes on the left and right sides of the ear, a total of 240 frequency domain features were obtained. Finally, this study used N = 36 cluster binning for all continuous EEG features to obtain discrete EEG features and merge them with the original EEG features. A total

of 480 ($4 \times 2 \times 30 \times 2$) EEG features were extracted. To reduce the potential impact of individual differences, this study used the Z-score normalization method to process the feature values between participants. All generated feature columns are in Table 1.

Physiological Signal	Feature Category	Feature Name	Explanation		
EEG	Frequency Domain Features $(\mu V^2/Hz)$	PSD	Energy distribution and intensity of the EEG signa in the δ , θ , α , and β wave frequency bands		
	Amplitude (µV)	AMP	Amplitude of the EEG signal in the δ , θ , α , and β wave frequency bands		
	Clustering Binning	EEG_36-bins	Discretization of continuous EEG features using $N = 36$ cluster binning		

Table 1. Description of generated features.

Feature Selection and Ground Truth

In this study, a feature selection method based on Logistic Regression (LR) and Recursive Feature Elimination (RFE) was used (Inza et al., 2004). This effectively reduced the number of features and improved the predictive performance of the model. After feature selection, based on the highest average accuracy of the five models, a total of 130 features were selected under the EEG modality.

This study used a video-based Take-Over Controllability (TOC) score to evaluate takeover performance (Naujoks et al., 2018), quantifying the driver's control ability during the takeover process. Our three raters underwent specialized training and gave an overall rating score $(1\sim10)$ by watching the takeover process videos. According to the evaluation process, the raters assessed whether the takeover was controllable, safe, or whether the takeover was good or even perfect. More detailed information and training materials can be obtained at www.toc-rating.de/en. In this study, scores of 1–3 were classified as high takeover performance, 4–6 as medium takeover performance, and 7–10 as low takeover performance. The final dataset obtained in this study included 199 high takeover performance labels, 206 medium takeover performance labels, and 108 low takeover performance labels.

Model Development

In order to construct a takeover performance prediction model, this study employed five machine learning algorithms, including DT, SVM, RF, Light-GBM, and MLP. These models excel in handling high-dimensional data and discovering complex patterns within the data, while also offering strong interpretability (Zhang et al., 2024).

Considering the quantity of existing data samples and previous research, this study chose the five-fold cross-validation method to train and compare the test results of the models. The hyperparameters of each model were also optimized. The training, testing, and evaluation of the algorithms in this study were all conducted in a Python 3.7 environment.

Model Evaluation

To evaluate the performance of the model, using a single evaluation metric is not comprehensive enough. Therefore, this study selected five commonly used evaluation metrics: Accuracy, Precision, Recall, F1-score, and Area Under the Curve (AUC), which are used to evaluate the performance of the takeover performance model. The AUC metric comes from the ROC curve, which is a useful tool for evaluating the performance of classifiers. For multi-category tasks, the confusion matrix is a k × k matrix, where the cell a_{ij} , $i, j \in$ [1, k] represents the frequency of samples with the true category C_i and the predicted category C_j . In addition, the metrics used to evaluate algorithm performance are defined as follows:

Accuracy =
$$\sum_{i=1}^{k} a_{ii} / \sum_{i=1}^{k} \sum_{j=1}^{k} a_{ij}$$
 (1)

Precision =
$$\frac{1}{k} \sum_{i=1}^{k} (a_{ii} / \sum_{j=1}^{k} a_{ij})$$
 (2)

Recall =
$$\frac{1}{k} \sum_{i=1}^{k} (a_{ii} / \sum_{j=1}^{k} a_{ji})$$
 (3)

$$F1 - score = \sum_{i=1}^{k} \frac{2 \times Precision(i) \times Recall(i)}{Precision(i) + Recall(i)}$$
(4)

For the best-performing model, its confusion matrix is analyzed to evaluate its specific performance in the takeover performance classification task. In addition, the Out-of-Bag Error (OOB) method of Random Forest is used to rank the importance of features (Gregorutti, Michel and Saint-Pierre, 2017). This technique helps to identify the most influential features in the takeover performance evaluation model.

RESULTS

To ensure the robustness of the machine learning models in this study, we conducted five-fold cross-validation using 43 different random seeds for each machine learning method under each time window. Firstly, this study used a paired T-test to compare the best machine learning model with the other four models, to determine whether LightGBM has the best performance. In

addition, this study analyzed the top fifteen most important features of the optimal model.

Model Evaluation

Under the EEG feature modality, the results of different models are shown in Figure 4. It can be observed that the MLP and LightGBM models achieved better model performance.



Figure 3: Accuracy, F1 score, and AUC values of five machine learning models.

Further, this study conducted a paired T-test on the predictive performance of the LightGBM model compared with the other four machine learning models. Table 3 shows that under a 20-second time window, the LightGBM model significantly outperforms the other four machine learning models in terms of accuracy, and significantly outperforms the DT, RF, and SVM models in terms of F1 score. The accuracy of the LightGBM model is 83.5%, and the F1 score reaches 82.1%.

Algorithm	Accuracy				F1-score			
	Mean	SD	t-test statistic	<i>p</i> -value	Mean	SD	t-test statistic	<i>p</i> -value
LightGBM	0.835	0.004	-	-	0.821	0.004	-	-
DŤ	0.585	0.005	278.53	< 0.001	0.570	0.005	244.24	< 0.001
RF	0.777	0.004	80.94	< 0.001	0.743	0.005	90.90	< 0.001
SVM	0.802	0.001	57.18	< 0.001	0.793	0.001	42.06	< 0.001
MLP	0.828	0.186	2.63	0.012	0.821	0.020	0.20	0.841

 Table 2. Comparison of average accuracy and F1 score of different models with the optimal model lightGBM under different time windows.

Confusion Matrix and Feature Importance Analysis

This section intends to conduct an in-depth analysis of the optimal model, LightGBM, obtained earlier. The confusion matrix of the optimal model with the best random seed of 19 is shown in Figure 5. The accuracy is 84.2%, the precision is 85.3%, the recall rate is 81.8%, the F1 score is 83.0%, and the AUC value is 95.2%. The results show that LightGBM has effectively learned the samples of medium takeover performance and high takeover performance. However, there are still some challenges in predicting samples with low takeover performance, with an accuracy of only 68.9%.



Figure 4: Confusion matrix of the lightGBM model with a time window of 20 seconds.

This study estimated the model feature importance through the OOB method of the random forest. Figure 6 shows the ranking of the top 15 feature importance in the driver takeover performance recognition model built based on EEG modality signals. The results show that 12 features come from the β band, and 3 come from the α band, indicating that for takeover performance prediction, the β and α bands play a more important role than the δ and θ band features. It is worth noting that the two most important features both come from the β band of the T8 channel. This may be due to the location of the T8 channel and the characteristics of the EEG physiological signals it records. The T8 channel is located on the right side of the scalp, close to the temporal lobe, which plays an important role in many cognitive and perceptual tasks. The EEG physiological signals of the β band are usually related to activities such as cognitive processing speed (Jenkinson and Brown, 2011). Therefore, the β band signal of the T8 channel may have captured important information about the driver's takeover performance.



Figure 5: The top fifteen important features with a time window of 20 seconds.

CONCLUSION

This study addresses the problem of predicting driver takeover performance in the context of conditional autonomous driving, using EEG signal features to construct a takeover performance prediction model. By comparing five machine learning models: DT, SVM, RF, LightGBM, and MLP, it was found that the LightGBM model performed best in predicting takeover performance, with an accuracy of 84.2% and an F1 score of 83.0%. In addition, the study also found that EEG features in the β and α bands play an important role in predicting takeover performance, especially the β band signals from the T8 channel, which contribute significantly to the prediction of takeover performance.

This study not only emphasizes the potential of machine learning models in predicting driver takeover performance, but also provides a new approach in the field of autonomous driving, i.e., using EEG features to assess the performance of drivers during the takeover process. This can help further optimize the design of autonomous driving systems, improving the safety and comfort of drivers during the takeover process. Future research can continue to explore more EEG features and other physiological and behavioral features in the application of takeover performance prediction, providing more comprehensive theoretical support and practical guidance for the development of the autonomous driving field.

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