

Connecting Image and Reality: The Role of 3D Printing in Surgical Planning

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ABSTRACT

Training the healthcare service members of tomorrow or assisting in the surgical planning of today's interventions is challenging, as the current CT/MRI images require an experienced and trained eye to interpret the intricate anatomy of the human body correctly. Although the CT/MRI scans are highly detailed and widely implemented, they cannot address the level of understanding a trainee or expert could gain through the hepatic perception or tactile learning experience offered by 3D printing. 3D printing enables hands-on understanding through highly detailed, patient-specific anatomical models from medical imaging, providing surgeons with an interactive way to visualise and practice complex procedures before entering the operating room. In surgical education, 3D-printed models, especially those simulating the texture of actual tissues or bones, provide essential tactile feedback that contributes to realistic training scenarios. This enhances surgical precision and reduces the likelihood of complications during surgery. Moreover, these models allow trainees to practice accurate replicas of human organs, improving their skills in a risk-free environment. Therefore, this paper presents a case study focusing on 3D printing in surgical planning that can effectively highlight the technology's current advantages and limitations. The models, fabricated with flexible and radiotransparent materials, allow surgeons to simulate surgical scenarios, improving preoperative planning, instrument handling, and decision-making. Subjective validation by specialists demonstrated that these models accurately replicate the physical properties of the target anatomy, aiding in better visualisation and procedural practice. However, limitations were observed in current methodologies, such as challenges related to material elasticity, the durability of 3D-printed models, and difficulties in navigating tortuous anatomical paths during simulations. Further, there is room for improvement in the accuracy of specific anatomical features and the interaction with surgical instruments, where minor irregularities hinder smooth operation. According to the findings, future work should focus on refining the materials used in 3D printing to enhance the robustness and realism of the models, particularly in complex anatomical structures. Additionally, incorporating real-time imaging data with 3D printing could further improve the adaptability of these models for preoperative simulations. Expanding these technologies beyond their current use in vascular surgery could revolutionise other surgical fields, offering customised, patient-specific planning tools across various medical disciplines.

Keywords: 3D printing, Surgical planning, Anatomical models, Tactile learning, Surgical training

INTRODUCTION

Two-dimensional (2D) images, such as X-rays, magnetic resonance images (MRI), or computerized tomography (CT) scans, have been and still are valuable tools in understanding different pathologies and the planning of surgical interventions (Thiruchandran *et al.*, 2025). In the early 2000s, the capability of turning 2D images generated by the listed medical image tools allowed the creation of complex, customized anatomical models first used to make dental implants and custom prosthetics (Lee Ventola, 2014). Since then, the application portfolio for 3D printing has evolved considerably. Applications like implant and tissue design, medical research, medical education and training, and surgical planning are exponentially growing (Lee Ventola, 2014; Tack *et al.*, 2016).

Through 3D printing, the process of how modern surgeons address surgical planning is changing. In 2016, Martelli *et al.* (2016) concluded that although the 3D printing technology had become more affordable and user-friendly, the cost and time to produce desirable outcomes would limit its widespread use in hospitals. The limitations were mainly related to the need for more guidelines on practical experience with 3D printing in surgery, resistance towards losing control over the decisions that affect their patients, and accepting external technical support. Almost a decade later, the landscape changes in 2025, Thiruchandran *et al.* (2025) present a collection of case studies on surgical planning split into two main areas: surgical guides based on 3D models of patient's anatomy and surgical instruments, 3D-printed instruments to assist with delicate procedures.

Therefore, modern surgical planning and training help to the limitations of CT and MRI, which require expert interpretation and lack tactile feedback crucial for skill development. 3D printing addresses these limitations by transforming imaging data into detailed, patient-specific anatomical models. These models enable interactive training and preoperative rehearsals, improving precision and reducing complications (Elkasabgy *et al.*, 2020; Thiruchandran *et al.*, 2025). This paper presents case studies highlighting 3D printing's advantages, including enhanced surgical planning and tactile stimulation, while addressing material properties and cost limitations. Recommendations are provided for integrating real-time imaging and expanding 3D printing to other surgical fields.

Traditional imaging techniques like CT and MRI are invaluable for visualising complex anatomical structures but need to offer the hands-on interaction required for comprehensive training and surgical planning. Lee Ventola (2014) estimated that in the next 10 years, the 3D printing healthcare industry will grow from \$11 million to \$1.9 billion worth of industry. This prediction was not fulfilled as it was way too conservative. Its estimate is 52% below the actual market size; according to Global Market Insights, the current healthcare 3D printing market size is \$2.9 billion (Healthcare 3D Printing Market Size and Share Report, 2030, 2024). In the next 10 years, 2032, the projected market value of 3D printing in healthcare applications is around \$13.8 billion. Other reports have a much more optimistic perspective of revenue forecasted in 2030, set at \$27.29 billion (*Healthcare 3D Printing Market Size & Share Report, 2032, 2024*).

Overall, it could be agreed that the forecast in revenue is, at least, as promising as the increasing number of case studies that highlight the utility of 3D-printed models in the healthcare sector. This paper explores 3D printing's transformative role in surgical education and planning, emphasising its current applications, challenges, and future directions.

Current Applications of 3D Printing in the Surgical Environments

Among the main medical applications for 3D-printed models of anatomical structures are educational applications, such as surgical training and simulation. Second, creating surgical instruments, therefore, preoperative planning applications. Last, patient-specific applications such as diagnosis and treatments (Winder & Bibb, 2005; Lee Ventola, 2014; Papotto *et al.*, 2022; Thiruchandran *et al.*, 2025). These applications underline the models' effectiveness in risk-free training environments and their contribution to better surgical outcomes (Webb, 2000; Rengier *et al.*, 2010).

In addition, 3D printed models help to enhance tactile learning by enabling the physical exploration of complex anatomies, which is critical for skill acquisition and confidence building. The 3D models fabricated from CT/MRI data replicate tissue textures, improving understanding of spatial and anatomical relationships (Mallon & Farnan, 2021; Thiruchandran *et al.*, 2025). Therefore, the application in surgical training and simulation can refine techniques and decision-making processes (Papotto *et al.*, 2022). Furthermore, such models support interprofessional education by facilitating collaborative learning in multidisciplinary teams, which is critical for optimising patient outcomes.

On the surgical preparation planning side, 3D printing has transformed the preoperative process by enabling the creation of custom surgical tools. These tools allow modern surgeons to perform specific procedures, or patient anatomies are now created rapidly and at a fraction of the cost compared to traditional manufacturing methods (Martelli *et al.*, 2016; Tack *et al.*, 2016; Elkasabgy, Mahmoud and Maged, 2020). The 3D printed tools enhance precision during surgery, minimising errors and reducing operation times. The orthopaedic and craniofacial surgeries, where exact measurements are critical, are a good case study for the use of 3D-printed guides to ensure proper alignment of instruments during the operative process (Wang *et al.*, 2020).

Lastly, 3D-printed models have also been shown to impact patient-specific applications for diagnosis and treatment significantly. In diagnostics, 3D-printed models enable clinicians to visualise and analyse complex anatomical anomalies in three dimensions, providing insights that may not be apparent in standard 2D imaging (Chen *et al.*, 2022). This is especially valuable in cases involving congenital abnormalities, intricate vascular conditions, or rare tumour locations (Mallon & Farnan, 2021).

Moreover, 3D-printed implants and prosthetics are becoming increasingly common for treatment (Hieu *et al.*, 2005; Bibb *et al.*, 2009). These patient-specific devices are designed to fit perfectly within a patient's anatomy, improving comfort and functionality. For example, custom cranial implants,

dental prosthetics, and orthopaedic devices have demonstrated superior outcomes to off-the-shelf alternatives (Lee Ventola, 2014). The technology also enables the creation of biocompatible materials and scaffolds for regenerative medicine, paving the way for future innovations in tissue engineering and organ printing (Mallon & Farnan, 2021).

Limitations and Challenges

While 3D-printed models are promising to enhance surgical preparation and decision-making, addressing the material and technological limitations is critical to advancing their clinical utility. From a technological perspective, current 3D printing methodologies face challenges in achieving the necessary resolution and accuracy to precisely replicate the organic anatomical structures. Fused Deposition Modelling (FDM), for instance, often results in layer lines that may interfere with the smooth surfaces required for particular medical simulations (da Silva *et al.*, 2021). Similarly, resin-based techniques such as Stereolithography (SLA) or Digital Light Processing (DLP) can produce high-resolution models. However, they may introduce brittleness due to the inherent properties of photopolymerised materials (Rashed *et al.*, 2024). Other technologies, such as Selective Laser Melting (SLM) and Selective Laser Sintering (SLS), excel in creating flexible and lightweight models with high resolution. However, high production costs (particularly for SLM), material limitations, and post-processing requirements hinder widespread adoption.

The post-processing aspect of 3D printed models adds another layer of limitations, as it involves additional steps that may introduce errors or inconsistencies (Shahrubudin *et al.*, 2020). Cleaning, curing, and finishing the printed parts can alter their dimensional accuracy and surface quality. These factors collectively hinder the scalability and practicality of 3D-printed models in routine clinical practice.

Regardless of such limitations, the potential of 3D printing in the healthcare sector becomes a valuable asset in the planning, simulation and training for complex interventions such as liver resections (Calle Gómez *et al.*, 2025), orthopaedic surgery (Koshkin *et al.*, 2024), fetal surgeries (Fils *et al.*, 2024) or craniofacial reconstructions (Park, 2022) to name a few cases. Ultimately, 3D-printed models fabricated with flexible and radio-transparent materials allow surgeons to simulate surgical scenarios, improving preoperative planning, instrument handling, and decision-making. Despite the advancements and benefits of 3D-printed models in medical applications, significant limitations persist due to the intricate demands of their use. One notable challenge lies in the inherent mechanical properties of the materials employed in additive manufacturing. Flexible and radio-transparent materials, while advantageous for surgical simulation, often lack the required mechanical strength and durability to endure repetitive or high-stress scenarios, limiting their long-term usability (da Silva *et al.*, 2021). Additionally, the elasticity of these materials may not adequately replicate the biomechanical properties of human tissues, which can impair the accuracy of surgical rehearsals (Rendas *et al.*, 2022). Therefore, developing

and validating 3D-printed models represent a cornerstone for pre-surgical planning and training for complex interventions.

Case Studies of Surgical Planning and Training

To overcome the limitations of 3D-printed models, developing and validating a model representing the aorta and its surrounding structures for pre-surgical planning and training in treating thoracic aortic aneurysms (TEVAR). The models were specifically designed to replicate anatomical conditions for TEVAR, which involve deploying prosthetic devices, such as stent grafts, into the aorta via femoral or transapical access. The prototype was designed to include the aortic valve, the aorta extending to the iliac bifurcations, and the left ventricle. Two variations of the left ventricle: one representing only the blood volume and another including the ventricular muscle, see Figure 1.



Figure 1: Thoracic aortic aneurysms 3D-printed model.

These models were fabricated using SLA (stereolithography) and RTV2 (room temperature vulcanising two components) silicon printing techniques. Flexible and semi-transparent resins were selected for the aortic structure. In contrast, elastic resins and silicone-based materials were used for the ventricular components to replicate realistic elasticity and transparency. The model also incorporated openings for femoral and transapical access, providing versatility for simulating different surgical approaches. To enhance functionality, design modifications were implemented after initial validation sessions. These included sealing internal iliac branches to facilitate water injection for lubrication and optimising the supports for robustness and ease of handling.

The model underwent a subjective validation process with surgical specialists at La Fe Hospital. Early assessments focused on material transparency, elasticity, X-ray transparency, and dimensional accuracy, see Figure 2.



Figure 2: Iterative validation process of the model with specialists and tests.

Iterative adjustments were made to accommodate surgical instruments and improve structural durability under manipulation. For instance, the iliac walls were thickened by 1.7 mm to allow smooth instrument insertion and redundant supports were removed to simplify handling surgical scenarios, demonstrating the model's efficacy in reproducing anatomical tortuosity and surgical challenges. The final prototype successfully allowed the deployment of prosthetic devices at targeted locations, validating its utility for training and planning, see Figure 3.

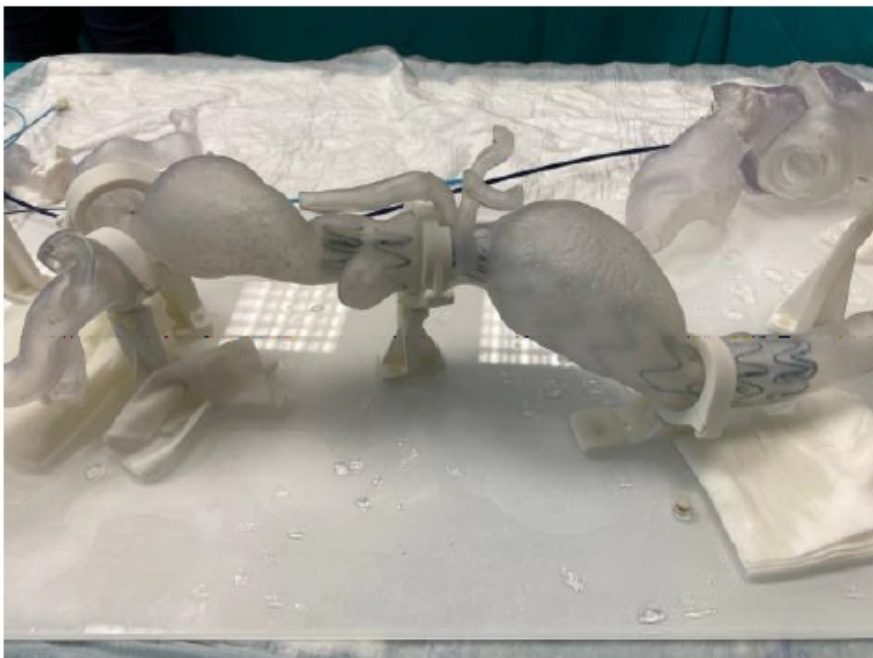


Figure 3: Deployment of prosthetic devices at targeted locations.

Future Directions

The development and validation of a 3D-printed anatomical model of the thoracic aorta and its surroundings have proven its potential in training vascular surgery and interventional radiology specialities. However, room for several improvements and research remains present.

Future model iterations could incorporate patient-specific anatomical data to enable personalised surgical simulations. By integrating imaging techniques such as computed tomography (CT) or magnetic resonance imaging (MRI), the models could provide more accurate anatomical representations tailored to individual cases. This advancement would enhance the realism and clinical applicability of the models in planning complex interventions such as the presented TEVR intervention.

Secondly, hybrid materials sections manufactured using RTV2 silicones with higher elasticity could be used to replicate human tissues' biomechanical properties better. While the current models demonstrated satisfactory elasticity and transparency, incorporating materials that simulate tissue response under physiological conditions could improve the fidelity of surgical simulations.

Expanding the model's scope to include additional anatomical regions, such as the ascending aorta and arch vessels, could enable simulations of more complex procedures. This expansion would address a broader range of surgical scenarios, including hybrid open-endovascular repairs.

By addressing these future directions, the resulting anatomical model could further improve surgical training, improve procedural outcomes, and ultimately contribute to better patient care in treating thoracic aortic aneurysms and related conditions.

CONCLUSION

In conclusion, the potential of combining 3D printing technology bridges the gap between traditional imaging and hands-on surgical training, offering detailed, patient-specific models for skill development and procedural training. To reinforce the statement, an innovative thoracic aorta and surrounding structures were presented as a training and preoperative planning tool for complex interventions such as thoracic endovascular aortic repair (TEVAR). This innovative model exemplifies how 3D printing and iterative design can advance surgical training and device testing. The insights gained from this project pave the way for developing more sophisticated and patient-specific models, potentially improving surgical outcomes and reducing risks in complex interventions. While challenges like material properties and cost remain, technological advancements and integration hold promise for broader medical applications.

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